



Wir schaffen Wissen – heute für morgen

Study of a compact curved superconducting dipole for the next generation of gantries at PSI using racetrack coils

(<u>C. Calzolaio</u>, S. Sanfilippo, M. Calvi, M. Negrazus, A. Gerbershagen, M. Schippers, M. Seidel)

17th-19th September, 2015

Superconductivity and other new Developments in Gantry Design for Particle Therapy Ciro Calzolaio



- Motivation;
- Magnet design using racetrack geometry;
- Nb₃Sn cable preliminary design;

Content

- Temperature increase due to a typical B cycle:
 - Dry magnet: cryocoolers;
 - Forced flow supercritical He (for comparison).
- Next steps.

18th September 2015

Motivation

- Proton therapy is a rapidly developing technique in cancer treatment.
- There is a global trend in the proton therapy research in reducing <u>size</u> and <u>weight</u> of the gantry, so reducing the <u>cost</u> of the future facilities.
- Use of superconducting magnet(s):
 - No large size effect (footprint & hight) has to be expected using superconducting magnets for proton therapy gantries.
 - The implementation of a final bend superconducting dipole is very useful to reduce the overall weight of the gantry.
 - A significant weight reduction leads to a significant reduction of the cost of the mechanical support structures. This cost benefit is tempered by the cryogenic costs.











Challenging specifications:

Main technical specifications for the dipole design:

- Bending angle: 45° (achromatic layout);
- Dipole curvature radius <1 m;
- Good field region (GFR): 250 x 250 mm²;
- Magnetic field in the GFR: 3 T;
- Field homogeneity in the GFR: $\leq 1\%$;
- Stray field at 1 m from the magnet exit ≤ 0.5 mT;
- Weight of the magnet < 10 tons;
- dB/dt = 0.1 T/s;
- The magnet has to rotate around the isocenter.

Magnet design using racetrack coils

The field quality has been evaluated calculating both the field homogeneity in the good field region (GFR) and the multipole decomposition.



5

Ciro Calzolaio

18th September 2015

Magnet design proposal using racetrack coils:

We want to keep the manufacturing as easy as possible.



The main multipole errors (along a circle of 250 mm diameter), the sextupole (n=3), the octupole (n=4), the decapole (n=5) and the seventh pole (n=7) are not exceeding 0.6% of the main field.



Active vs passive shielding (1)



We tried different passive shielding options.

A passive shielding system alone does not allow to have 0.5mT at the patient location preserving the magnet mass below 6000 kg.

18th September 2015

Superconductivity and other new Developments in Gantry Design Ciro Calzolaio for Particle Therapy

Active vs passive shielding (2)

Coils mounted on the treatment room walls.



The current in each coil has to be changed as a function of the rotation angle. Here in the simulations:

Angle	Current Top	Current Bottom	Current Left	Current Right	Dipole	Shaping
0°	24 A/mm ²	24 A/mm ²	0 A/mm ²	0 A/mm ²	73.8 A/mm ²	-64.6A/mm ²
45°	2 A/mm ²	-15 A/mm ²	3 A/mm ²	14 A/mm ²	82.0 A/mm ²	-61.5A/mm ²
18th September 2015Superconductivity and other new Developments in Gantry DesignCiro Calzolaio						8

Active vs passive shielding (3)

The shaping coils (the racetrack coils arranged aside with respect to the main dipole) allows to:

- enhance the field quality in the GFR;
- reduce the stray field at the patient location. The shaping coils alone do not allow reaching the specifications in terms of stray field though. Specification: 0.5mT @ 1 m from the magnet exit.



racetrack coils and the split solenoid:

- B=0.4 mT @ patient locations;
- Total mass: 1620 kg.



Ciro Calzolaio



18th September 2015



PAUL SCHERRER INSTITUT **Superconducting strand: a proposal**



60

Strand Φ	0.82 mm	
Filaments twist pitch	~ 14 mm	
n. filaments	8305	
n. Bundles	151	
n. Filaments per bundle	55	
Filaments Φ	6-8 μm	
Cu/non Cu	0.93	
Ic @ B=4.5 T, T=4.2K, ε=0.2%	200.5 A	

Strand performance @ 19 T, 4.2 K no bending: Bruker EAS no bending: Bruker EAS Bochvar & ChMF Bochvar & ChMP 0.4 % bending: Bruker EAS



18th September 2015

Superconductivity and other new Developments in Gantry Design Ciro Calzolaio for Particle Therapy

Hot spot temperature after quench (1)

In order to calculate the amount of copper to be used in the winding pack $(Nb_{3}Sn)$, the hot spot temperature (T_{M}) was estimated simulating a quench of the magnet.

The behaviour of T_M with the winding pack composition was then analyzed.



At least 40% of Cu is necessary in the winding pack to avoid too high hot spot temperature in case of quench.

18th September 2015

Hot spot temperature after quench (2)





17th September 2015

Superconductivity and other new Developments in Gantry Design Ciro Calzolaio for Particle Therapy

AC loss estimation for the superconducting cable



AC loss estimation for the superconducting cable



Superconductivity and other new Developments in Gantry Design for Particle Therapy

Ciro Calzolaio



18th September 2015

PAUL SCHERRER INSTITUT

Cooling system 1: cryocoolers

We would need flexible lines:

- To avoid the compressor to be mounted on the rotating gantry;
- To reduce the vibrations transmitted to the winding pack;
- Long flexible lines result in performance reduction but work as well as reservoir.

Sumitomo Heavy Industries, ltd. 40-50 k€

Compresso



 If the cold head rotates, a cooling power decrease has to be considered: ~10% from 0° to 90°

It would be much better if we could work at around 20 K!!!

Cu thermal path for heat distribution



PAUL SCHERRER INSTITUT

Cooling system 1: cryocoolers



PAUL SCHERRER INSTITUT

Cooling system 1: cryocoolers



Superconductivity and other new Developments in Gantry Design for Particle Therapy 20

Ciro Calzolaio

Cooling system 1: cryocoolers

Cool-down may take a while....

PAUL SCHERRER INSTITUT



Cooling system 2: forced flow supercritical He (1)



Superconductivity and other new Developments in Gantry Design Ciro Calzolaio for Particle Therapy

Cooling system 2: forced flow supercritical He (2)



He mass flow rate	5 g/s
He inlet pressure	0.4 MPa
He inlet temperature	4.5 K

18th September 2015

Cooling system 2: forced flow supercritical He (3)





He pressure (MPa)



Cooling system 2: forced flow supercritical He (3)





He pressure (MPa)



Cooling system 2: forced flow supercritical He (4)

Magnet temperature evolution (K)



Mechanical supports

18th September 2015

The forces on the winding pack were calculated in the OPERA 3D model: the highest forces were found on the south (S) dipole coil. I considered the mechanical support for this coil.



Superconductivity and other new Developments in Gantry Design Ciro Calzolaio for Particle Therapy

Mechanical supports

The forces on the winding pack were calculated in the OPERA 3D model: the highest forces were found on the south (S) dipole coil. I considered the mechanical support for this coil.



Mechanical supports: von Mises stress calculation

For structural material and welds, the limiting stress for plastic collapse (equivalent to the 'limiting stress intensity' value) at design temperature is usually defined as $2/3 \sigma_y$. Special care has to be used especially in all the connection parts.





Mechanical supports: von Mises stress calculation

For structural material and welds, the limiting stress for plastic collapse (equivalent to the 'limiting stress intensity' value) at design temperature is usually defined as 2/3 σ_y . Special care has to be used especially in all the connection parts.



Mechanical supports: von Mises stress calculation

For structural material and welds, the limiting stress for plastic collapse (equivalent to the 'limiting stress intensity' value) at design temperature is usually defined as 2/3 σ_y . Special care has to be used especially in all the connection parts.



18th September 2015

Superconductivity and other new Developments in Gantry Design Ciro Calzolaio for Particle Therapy



Conclusions

- A magnet geometry with 4 coils + active shielding (4 coils) allows to fulfill the specifications without using an iron shield.
- A bronze routed Nb₃Sn strand has been considered for the dipole magnet winding;
- Rutherford cables may be used to wind the magnet;
- Cooling system may be a challenge as the magnet has to be cycled and it has to rotate around the patient.
- Cooling by means of cryocoolers may be problematic (unless a large number of units is employed and/or a dB/dt as lower as <u>0.05-0.1T/s</u>).
- Forced flow would be effective but extremely challenging (and expensive).
- A detailed model of AC losses is mandatory to design (and optimize) the cryogenic system.
- Using Nb₃Sn at low current density may provide a large temperature margin $(\sim 5 \text{ K})$ that can cope with the temperature increase due to AC losses.



- Detailed cable model for AC losses calculation: Collaboration with University of Bologna;
- Cryogenic design study;
- Mechanical structure design;
- Cost estimation.

Thank you for the attention

APPENDIX



AC loss: hysteresis in the filaments



Superconductivity and other new Developments in Gantry Design Ciro Calzolaio for Particle Therapy

AC loss: coupling in the strand

• Strand coupling (at low frequency);





Cable coupling (at low frequency);



Dynamic resistance

A dynamic resistance appears against transport current, causing an increase in AC loss

$$K_{dR} \approx \left(1 + \left(\frac{I_{op}}{I_c}\right)^2\right)$$

$$E_{\perp} = \frac{1}{3} \frac{wL_p}{t} \left(\frac{N^2}{20R_c} + \frac{1}{R_a} \right) \Delta B_{\perp} \dot{B}_{\perp}$$

Adjacent



Cooling system 2: forced flow supercritical He (4)







Superconductivity and other new Developments in Gantry Design Ciro Calzolaio for Particle Therapy