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Analog Signal Processing for Particle Detectors

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Citation of a slightly dispirited assistant I met during the early days of my studies:

"If you need an amplifier then try to build an oscillator, I am sure it will never oscillate, but if you need an oscillator then try to build an amplifier..."

Of course this statement is not true, but there are a couple of reasons why an oscillator may not oscillate whereas an amplifier does.



Analog Signal Processing for Particle Detectors

Topics

- analog signal processing
- charge and current preamplifier
- pulse shaping
- examples



Analog Signal Processing for Particle Detectors



Mostly linear treatment of weak currents caused by small charges deposited or generated within a detector

Its goal is the extraction of information out of the weak generally noisy signals with the best possible S/N-ratio and/or the lowest possible timing jitter

It includes at lest three steps:

- signal capturing and (pre-)amplification
- pulse shaping by bandwidth manipulations
- signal conditioning for the following stage



Ch1(yellow):signal after pulse shaping Ch2(blue): signal e.g. after a charge sensitive preamplifier



Analog Signal Processing

Keywords in Analog Signal Processing are:

- Gain
- Bandwidth
- Dynamic input/output range
- Stability
- Linearity
- Pulse shaping/Filtering
- Noise
- Distortion
- Drive strength
- Powering and grounding scheme
- Power consumption and cooling
- Mechanical considerations (housing, size, integration)

Not covered in the above list are topics specific for **non-linear analog processing** (e.g. frequency mixing as it is usual done in RF-communication, ...)



Analog Signal Processing

What has to be known to be able to develop a signal processing chain

from the experiment:

- parameters to be measured (energy, position, intensity, time of arrival, counts, ...)
- expected hit rate and their time distribution (poisson, bunch,...)
- other particles giving signals which has to be suppressed (e.g. by energy evaluation)
- environment conditions(magnetic fields, vacuum,)

from the detector:

- amount of charge deposited
- charge collection time
- detector recovery time
- detector capacitance and resistivity
- part of signal containing information
- readout scheme (e.g. charge division, time delay, ...)
- number of channels
- operating voltage



Analog Signal Processing

What has to be known to develop a signal processing chain

• from the next DAQ stage:

- type of stage (discriminator, counter, TDC, ADC, ...)
- input type (single ended, differential)
- input voltage or current range
- bias point
- input impedance
- input bandwidth or sampling frequency (for analog signals)
- minimum pulse width (for digital signals)



Applicable for Measurements of Energy deposited on detector

 $E_{particle} \propto Q_s = \int^{\tau} i_s(t) dt$ with $\tau >> T_{charge_collection}$

typical dynamic range: $\frac{Q_{s_max}}{Q_{s_min}} = 10^3 \dots 10^5$ (= 60 \ldots 100 dB or = 10...17 bits)

Energy information is a charge => Integration of current is needed

Charge sensitive preamplifier:

The most common ways are either to use a charge sensitive preamplifier based on a operational amplifier or especially when there is a cable in between detector and preamplifier a resistor with the cable impedance followed by a voltage amplifier:





Preamplifier for Charge Measurements

Charge Sensitive amplifier using an operational amplifier:

Operational Amplifier:

Open loop gain $dV_{out}/dV_{in} = -A$ ($|A| \approx 1E3-1E4 >> 1$) Input resistance $R_{in} \approx 10 - 100 \text{ M}\Omega$ (or even higher) Negative feedback forces $V_{in} \approx 0$ (but not = 0) => partial charge transfers from C_d to C_f

Reason for the only partial transfer:

Amplifier transforms the feedback capacitor C_f into a dynamic input capacitance

$$C_{in} = \frac{Q_{in}}{V_{in}} = \frac{C_f \cdot V_f}{V_{in}} = \frac{C_f \cdot V_{in} \cdot (A+1)}{V_{in}} = C_f (A+1)$$

=> Free charges from the detector are divided on both capacitances (C_d and C_{in}) with the

ratio: $v_{in} = Q_d/C_d = Q_{in}/C_{in} \implies Q_d = Q_{in} \cdot C_d/C_{in}$ and $Q_{tot} = Q_d + Q_{in} = Q_{in}(C_d/C_{in} + 1)$

$$\Rightarrow \quad \frac{Q_{in}}{Q_{tot}} = \frac{1}{\left(\frac{C_d}{C_{in}} + 1\right)}$$

Charge sensitivity of the amplifier: $A_{VQ} = \frac{V_o}{Q_{in}} = \frac{-A}{A+1} \cdot \frac{1}{C_f} \approx -\frac{1}{C_f} \left[\frac{V}{C} \right]$



Attention: this circuit will not



Preamplifier for Charge Measurements



has an exponential slope (dU~e $-t/\tau$)

comparator with hysteresis switching the transistor on after V_{out} reaches a certain level

generates unpredictable dead-times

may be harder affected by temperature variations than resistor



Dynamic Range of Amplifiers

Dynamic Range of Amplifiers:

Ratio between largest (S_{max}) and smallest (S_{min}) signal for which the amplifier works within its specifications

It is typically expressed in [dB]: $DR = 20 \cdot log_{10} \left(\frac{S_{max}}{S_{min}}\right)$ [dB]

Rem: The dynamic range can be expressed for output or input signals. In a perfect linear system it would be the same.

For precision measurement systems:

The specification of a minimum S/N-ratio and enhanced linearity requirements reduce the available dynamic range of the system.





Applicable for event counting at high counting rates

Remark: Current preamplifier (also called transimpedance amplifier) are not faster but they have almost no tail what makes their signals shorter

Characteristics:

- Best for high counting rates
- poorer noise performance compared to charge sensitive preamplifiers
- more affected by stability issues especially for detectors with high detector capacitance

Transimpedance preamplifier (TIA):

the working principle is quit similar than for the charge amplifier except that the the feedback resister can not store charges

=> the main topic here is stability





Preamplifier for Current Measurements





Pulse Shaping - Objectives

Reasons for pulse shaping:

- Shaping towards increased pulse width:
 - => Bandwidth-reduction
 - Improve of Signal-to-Noise Ratio
 - Pulse conditioning to match next stage requirements (e.g. stretching & rounding of sharp peaks for amplitude measurement with an ADC at a given f_{sampling})
- Shaping towards reduced pulse width
 - => Improve of Pulse Pair Resolution (pile-up reduction):
 - Increase of maximum count-rate
 - Minimization of energy-measuring errors
 - Dead-time or dead time variation reduction
- Other, sometimes included objectives:
 - Reduction of baseline problems
 - Minimization of timing errors

Conflicting objectives (e.g. best S/N-Ratio at max. count-rate):

=> "Optimum shaping" is usually an application dependent compromise and has to be specified!









Most common pulse shaping methods:

- 1. CR-RC Pulse Shaping
- 2. Pole-Zero Cancellation
- 3. Delay-Line Pulse Shaping
- 4. Gaussian Filter
- 5. Raised-cosine Filter
- 6. Sinc Filter
- 7. Constant Fraction Discriminator
- 8. Baseline Restorer

Blue = subjects in tis talk



1. CR-(RC)ⁿ Pulse Shaping:





1. CR-(RC)ⁿ Pulse Shaping:







CR - Pulse Shaping ("differentiator"):



step response:

$$h(t) = \frac{V_{Dout}(t)}{V_{step}(t)} = e^{-\frac{t}{R_D C_D}}$$

Design limits for R_D:

- a lower limit for R_D is given by the max. output drive current of the previous amplifier stage and their maximum peak to peak output voltage
- to be dominant, R_D should be big compared to the output impedance of the previous amplifier



reduces pulse width if RC << T, but has inconveniences:

- Generates bipolar output pulses (positive on rising edges and negative on falling edges) => only applicable if falling edge has a much longer time constant
- Peak at maximum amplitude is very short in time (bad e.g. for ADC-sampling)



CR - Pulse Shaping ("differentiator"):



step response:

$$h(t) = \frac{V_{Dout}(t)}{V_{step}(t)} = e^{-\frac{t}{R_D C_D}}$$

transfer function:

$$G_D(s) = \frac{V_{Dout}(s)}{V_{Din}(s)} = \frac{sC_DR_D}{1 + sC_DR_D}$$

Frequency domain characteristics





RC - Pulse Shaping ("integrator"):



step response:

$$h(t) = \frac{V_{Iout}(t)}{V_{step}(t)} = (1 - e^{-\frac{t}{R_I C_I}})$$

Time domain characteristics





RC - Pulse Shaping ("integrator"):



step response:

$$h(t) = \frac{V_{Iout}(t)}{V_{step}(t)} = (1 - e^{-\frac{t}{R_I C_I}})$$

transfer function:

$$G_{I}(s) = \frac{V_{Iout}(s)}{V_{Iin}(s)} = \frac{1}{1 + sC_{I}R_{I}}$$

Frequency domain characteristics



frequency [Hz]







CR-RC Pulse Shaping-mathematical intermezzo: Derivation of h(t) for the case where $\tau_D = \tau_1$:

Starting point is the previous general formula for the CR-RC step response:

$$h(t) = \mathcal{L}^{-1}\left\{\frac{G_{DI}(s)}{s}\right\} = \frac{v_{out}(t)}{v_{step}(t)} = \frac{\tau_D}{\tau_D - \tau_I} \cdot \left(e^{-\frac{t}{\tau_D}} - e^{-\frac{t}{\tau_I}}\right)$$

As the above formula for $\tau_D = \tau_1$ apparently results in a zero divided by zero division, a limes calculation with $\Delta \tau = \tau_D - \tau_1 \rightarrow 0$ may help:

$$h(t) = \lim_{\Delta \tau \to 0} \left(\frac{\tau_D}{\tau_D - \tau_I} \cdot e^{-\frac{t}{\tau_D}} \cdot (1 - e^{-t\left(\frac{1}{\tau_I} - \frac{1}{\tau_D}\right)}) \right)$$
 factored out $e^{-\frac{t}{\tau_D}}$

 $= \tau_D \cdot e^{-\frac{t}{\tau_D}} \cdot \lim_{\Delta \tau \to 0} \left(\frac{1 - e^{-t \left(\frac{\tau_D - \tau_I}{\tau_I \tau_D}\right)}}{\tau_D - \tau_I} \right)$ some minor cosmetics

$$= \tau_D \cdot e^{-\frac{t}{\tau_D}} \cdot \lim_{\Delta \tau \to 0} \left(\frac{\frac{d}{d\Delta \tau} (1 - e^{-t \left(\frac{\Delta \tau}{\tau_I \tau_D}\right)})}{\frac{d}{d\Delta \tau} (\Delta \tau)} \right)$$
 l'Hospital's rule

$$= \tau_D \cdot e^{-\frac{t}{\tau_D}} \cdot \lim_{\Delta \tau \to 0} \left(\frac{t}{\tau_I \tau_D} \cdot e^{-t\left(\frac{\Delta \tau}{\tau_I \tau_D}\right)} \right) = \frac{t}{\tau_I} \cdot e^{-\frac{t}{\tau_D}} = \frac{t}{\tau} \cdot e^{-\frac{t}{\tau}} \qquad \text{limes, then } \tau_I = \tau_D = \tau$$







1. CR-(RC)ⁿ Pulse Shaping:



Increasing number of integrators make the output Pulse more symmetrical wit a faster return to base-Line.

To preserve the peaking time the time constant of the original integrator (for n=1) has to be divided by the number n: $\tau_n = \tau_1 / n$





- 2. Pole-Zero Cancellation:
- Controls the lower cutoff frequency
- No impact on the upper cutoff freq.
- Can be used for pulse shape and baseline recovery adjustments
- It is not the most efficient but an easy to integrate shaper



Application:

Charge sensitive amplifiers and stabilized transimpedance amplifiers (with a capacitance in their feedback) have a pole at $s=1/C_FR_F$ in their transfer function.

This pole can be compensated with the above circuit (yellow part) which creates a zero. To compensate the pole one has to choose: $C_{PZ} \cdot R_{PZ} = C_F \cdot R_F$

The value of the Resistor R_x has no effect on the zero except it would be zero or infinite.

=> pole zero cancellation can be applied as well in other networks for pulse shape and baseline optimization (e.g. for AC-coupled signal paths)



2. Pole-Zero Cancellation:

In frequency domain:

in time domain:





Some Examples



Conceptual study POLDI-Upgrade







Pictures below: Hildebrand, Stoykov, Mosset







Schematics of the Input Amplifier:





Charge Division Readout – Track and Hold Stage





Example: MAR-Amplifier

MAR-Amplifier for Photon-Detectors



The two gain stage amplifier design includes:

- π-attenuator for gain setting
- · adjustable pole-zero cancellation for pulse shaping
- integrating capacitor for upper bandwidth limitation
- lower bandwidth adjustment by of AC-coupling capacitor
- · filtered high voltage path for reverse bias voltage

Typical application scheme:



Specifications (with MAR-6SM on both stages):

- Input impedance 50 Ω
- primary transimpedance gain 50 V/A
- 50 V//
- voltage gain (with no π attenuation):

Frequency	100 kHz	750 MHz	1 GHz	2 GHz
Gain	40 dB	37 dB	32 dB	22 dB

- linear output range (1dB compression) 342 mV_{rms} @ 50Ω

- max. reverse bias voltage 200 V
- power-consumption amplifier

+12 V, 32 mA

Functional description:

The "MAR"-Amplifier was designed for fast photo-diode (e.g. APD) applications where due to limited space at the detector-side the photo-diodes has to be off-board and where coax cables are needed to connect them to the amplifiers.

The board layout allows for the assembly of two RF gain blocks which can be chosen from a wide palette of monolithic amplifiers in .085 micro-x or SOT-89 case styles.

Within 50 Ω systems the amplifier can be used either as transimpedence or voltage amplifier. It is cascadable.



Example: MAR-Amplifier

The MAR-Amplifier







MAR-Amplifier for STXM @ PolLux-Beamline



Brief description:

Amplifier for fast avalanche photo diodes (e.g. Silicon Sensor, AD230-8, 180 ps rise time) with integrated low and high voltage filters, a current monitor output for the APD bias current and pulse-shaping options like a π -attenuator, an integrating capacitor and a pole-zero cancellation stage.

The board layout allows to read out the APD-signal either on the cathode or anode side. The two RF amplifier stages can be assembled with a wide palette of monolithic amplifiers in .085 micro-x or SOT-89 case styles.

Specifications (MAR-6SM on both stages):

RF-Amplifier Output:

- current to voltage conversion 50 V/A

- voltage gain at frequency

Frequency	100 kHz	750 MHz	1 GHz	2 GHz
Gain	40 dB	37 dB	32 dB	22 dB

- max. output voltage (1dB Comp): 282 mV @ 50Ω

Current Monitor Output:

- input current range 0...500 nA < 0.1% full scale
- accuracy
- current to voltage conversion
- bandwidth 1 kHz

Power-Supply:

- Amplifier +/-12V, 300mA - max. APD - voltage 200 V

1 V/µA



MAR-Amplifier for STXM @ PolLux-Beamline





Static imaging and 1st movie of magnetization dynamics taken with the new APD-Detector at the PolLux-STXM



APD-Detector : Urs Greuter, Blagoj Sarafimov, Jörg Raabe, Aleksandar Puzic



Principle of detection and data acquisition

Slide received on 24.06.2010 from Jörg Raabe

Sample: Co (50 nm) / Rh (0.75) / NiFe (50 nm) FM coupling due to Ne ion irradiation



Ni 859.2 eV

Co 783.7 eV



static magnetic imaging: square 2000 nm x 2000 nm, P+/P-

movie: square 1000 nm x 1000 nm image size: 1000 nm x 1000 nm resolution: 15 nm dwell time: 20ms 2 phases (0 deg & 45 deg) with 4 channels

measured magnetization component: out-of-plane (vortex core) Ni (859.2 eV), P-

Excitation: f = 625 MHz, $B_0 = 2.25$ mT (in plane) field







Sample preparation: Sebastian Wintz, Thomas Strache